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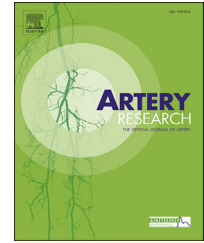
Validation of non-invasive central blood pressure devices: Artery society task force (abridged) consensus statement on protocol standardization

James E. Sharman, Alberto P. Avolio, Johannes Baulmann, Athanase Benetos, Jacques Blacher, C. Leigh Blizzard, Pierre Boutouyrie, Chen-Huan Chen, Phil Chowienczyk, John R. Cockcroft, J. Kennedy Cruickshank, Isabel Ferreira, Lorenzo Ghiadoni, Alun Hughes, Piotr Jankowski, Stephane Laurent, Barry J. McDonnell, Carmel McEniery, Sandrine C. Millasseau, Theodoros G. Papaioannou, Gianfranco Parati, Jeong Bae Park, Athanase D. Protogerou, Mary J. Roman, Giuseppe Schillaci, Patrick Segers, George S. Stergiou, Hirofumi Tomiyama, Raymond R. Townsend, Luc M. Van Bortel, Jiguang Wang, Siegfried Wassertheurer, Thomas Weber, Ian B. Wilkinson, Charalambos Vlachopoulos

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Validation of non-invasive central blood pressure devices: Artery society task force (abridged) consensus statement on protocol standardization



KEYWORDS

Guideline;
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Abstract Brachial cuff blood pressure (BP) is clinically important, but may be an inaccurate substitute for central BP. Many non-invasive devices have been developed that purport to estimate central BP from peripheral artery sites, yet with no standardized guidelines; the accuracy testing of these new devices has not been undertaken in a uniform fashion with comparable protocols. This is an abridged paper describing the recommendations reached by an international task force convened to identify issues that need to be addressed and reach consensus relating to methods for assessing and reporting the accuracy (validation) of central BP devices. The recommendations are endorsed by the Association for Research into Arterial Structure and Physiology (ARTERY) Society, as well as the European Society of Hypertension (ESH) Working Group on Arterial Structure and Function, and the ESH Working Group on Blood Pressure Monitoring and Cardiovascular Variability. Researchers interested in validating central BP monitors should read the full version of the statement.

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Introduction

The original Riva-Rocci method to measure blood pressure (BP) using a cuff at the upper arm assumed the pressure obtained by this technique was a good proxy for central aortic BP.^{1,2} The clinical (prognostic) importance of brachial cuff BP is undeniable for both the assessment of cardiovascular risk associated with elevated BP and the benefits of treatment-induced BP reduction.³ However, it is also generally appreciated that peripheral artery systolic BP (SBP; brachial or radial artery) may be an inaccurate substitute for central SBP.⁴ This has been reported in human studies using intra-arterial catheterization of peripheral and central arteries.^{5–8} There may also be a discrepancy between peripheral and central BP responses to vasoactive drugs.⁹ These findings are corroborated in

larger studies using non-invasive central aortic BP methods,^{10–13} and, while yet to be fully adopted in clinical practice, an independent prognostic value of central BP has been demonstrated.^{14–16} Altogether, there is a growing interest among clinicians toward improving risk estimates by using devices that provide more accurate measures of central aortic BP than those provided by current brachial cuff BP methods.

Many non-invasive devices have been developed that purport to estimate central BP from different peripheral artery sites (e.g. radial, brachial, carotid arteries) using different principles of recording the pressure or surrogate signals (e.g. applanation tonometry, oscillometry, ultrasound or magnetic resonance imaging) and different calibration methods to derive central BP. Since upper arm cuff-based devices to estimate central BP are more clinically appealing, in recent years several companies have

developed such devices using a variety of techniques (e.g. oscillometric sub-diastolic or supra-systolic waveform analysis with generalized transfer functions), which employ a variety of signal processing steps to estimate central BP from peripheral signals.^{17,18} Yet, with no standardized guidelines,¹⁷ the accuracy testing of these new devices (as well as the preceding devices) has not been undertaken in a uniform fashion with comparable protocols, emphasizing the need for guidance in this field.^{19–22} An international task force was convened to address this situation.

Task force aims

1. To identify issues that need to be addressed and reach consensus relating to methods for assessing and reporting the accuracy of central BP devices.
2. To provide recommendations regarding appropriate protocols to assess and report the evaluation of accuracy (validation) of central BP devices.

The full report of the task force was recently published²³ and in this abridged version, the majority of information is presented in summary format within Tables. Table 1 gives a glossary of terms and a summary of issues and recommendations is provided in Table 2. A summary of differences between device types in comparison to intra-arterial brachial and central aortic BP are presented in Fig. 1. Researchers interested in validating central BP monitors should read the full version of the statement.²³

Validation protocol requirements

Several scientific bodies have developed validation protocols for non-invasive peripheral BP monitors,^{24–29} yet they differ on procedural features such as sample size and selection criteria, number of assessment phases, acceptable margin of error, BP range and pass/fail criteria.³⁰ A 'universal' brachial BP validation protocol has been developed through collaboration of the American Association for the Advancement of Medical Instrumentation (AAMI), the

Table 1 Glossary of terms.

Intra-arterial (invasive) blood pressure	Direct measurement of blood pressure within the artery using an in-dwelling catheter-based pressure transducer.
Peripheral (non-invasive) blood pressure	Blood pressure at a site distal from the aorta. This most often refers to brachial or radial artery blood pressure, but for the purpose of this paper also includes carotid blood pressure even though local derivation is regarded as a surrogate of central blood pressure.
Central (aortic) blood pressure	Blood pressure in the proximal ascending aorta.
Systolic blood pressure amplification	The increase in systolic blood pressure from proximal to peripheral arterial vessels (e.g. aorta-to-brachial, or brachial-to-radial arteries).
Transfer function	Signal processing step to estimate central blood pressure waveforms from peripherally recorded waveforms.
Calibration	Process of scaling a waveform using units of pressure.

Table 2 Summary of issues in the assessment and reporting of central blood pressure (BP) monitors and recommendations.

Issue	Recommendation
1. Disparity of non-invasive central BP devices as to what is being measured	Device manufacturers should clearly state the purported measurement function of their device. These can be broadly categorized into two types based on function: Type I – estimates central BP relative to measured brachial BP; Type II – estimates intra-arterial central BP. Both function types may be available within a single device.
2. Calibration of peripheral artery signals using brachial cuff BP	To achieve accurate non-invasive assessment of true central BP, more accurate non-invasive estimates of intra-arterial brachial BP are needed. Establishing more rigorous accuracy criteria for brachial BP is desirable. Current evidence suggests that calibration with MAP and DBP may provide a more accurate assessment of central BP than calibration with SBP and DBP.
3. Disparity in validation standards	The reference standard against which device accuracy of central BP estimation is gauged should be intra-arterial catheter in the ascending aorta. Details of the calibration method should be provided. If the brachial BP waveform undergoes recalibration to produce a 'new' brachial BP, then the recalibrated brachial BP values (and the method to derive them) should also be provided so that the level of estimated aorta-to-brachial systolic BP amplification can be gauged.
4. Limitations in performing invasive validation studies	In future, it may be reasonable to use non-invasive central BP devices as reference standards, but the acceptance criteria for this are yet to be determined.

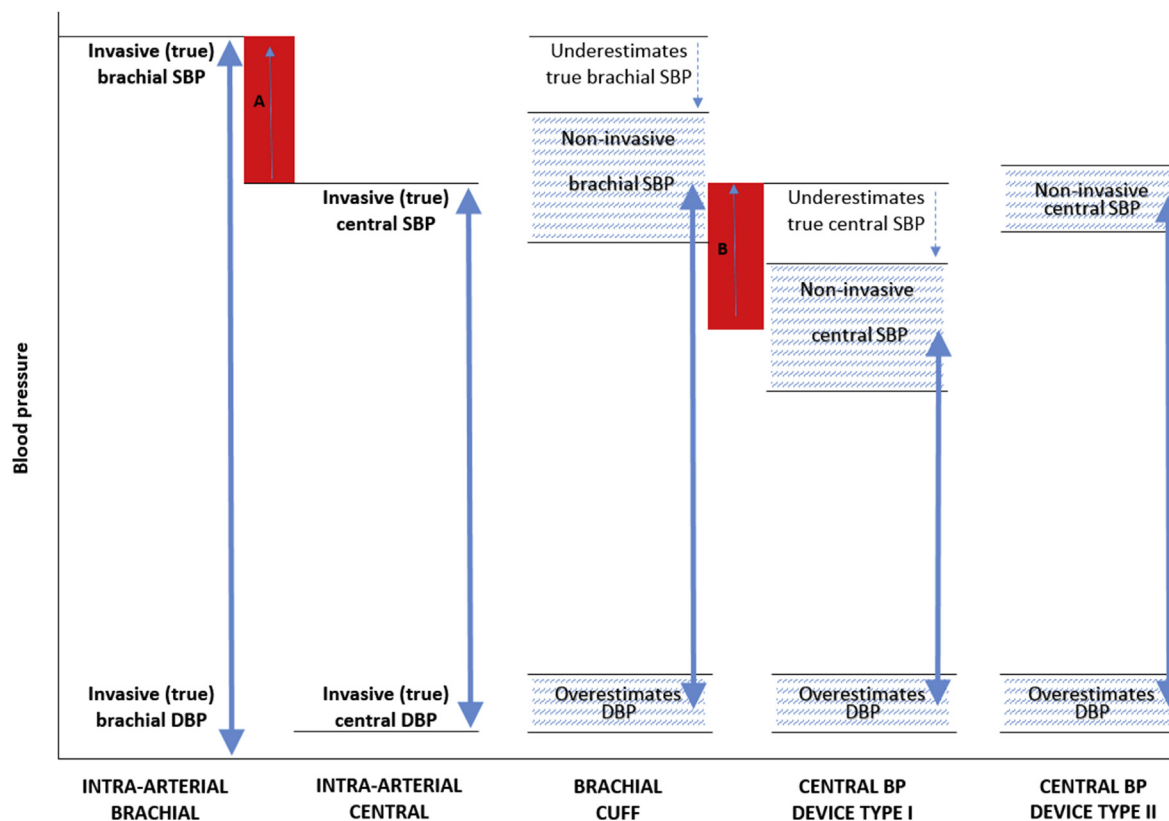


Figure 1 Illustration of the differences in systolic (SBP) and diastolic (DBP) blood pressure (BP) between intra-arterial brachial and central BP, brachial cuff BP and non-invasive central BP devices Types I and II (BP ranges of different methods represented by the double arrows). Red shaded area A, represents the true (intra-arterial) level of central-to-brachial SBP amplification, and red shaded area B represents the non-invasive estimated central-to-brachial SBP amplification (A and B may be similar in magnitude). The non-invasive central SBP estimated using central BP device Type II may be higher than non-invasive brachial cuff SBP, but this is due to underestimation of true (intra-arterial) brachial SBP with the cuff device and, therefore, does not reflect physiological amplification. The hatched areas denote that there will be a degree of variability in estimated BP between devices. Reproduced from Sharman et al.²³ with permission.

International Organization for Standardisation (ISO) and the ESH Working Group on Blood Pressure Monitoring and Cardiovascular Variability, and projected to be in effect in 2019.³¹ This harmonised protocol is expected to inform many aspects of central BP validation protocols that equally apply to brachial BP (e.g. age, gender, BP range), but an internationally accepted central BP protocol directed by regulatory authorities is still required, as distinct from the forthcoming brachial BP protocol.

Recommendations focus on central BP specific protocol requirements, with some relevant features drawn from existing validation guidelines.^{24–26} For unambiguous interpretation of requirements, facets of the protocol have been listed in terms of “must,” “should” and “may.” “Must” indicates a necessary component for highest quality, “should” indicates a strong recommendation, but may not be the only way that the component can be achieved, and “may” is used to provide further guidance. Protocol requirements are summarised in Table 3 as a pro-forma guide for investigators. Less attention is given to protocol features equally relevant to brachial BP (i.e. sample

characteristics, results reporting and pass criteria) but some proposed direction is also provided based on existing guidelines^{24–26} for interim guidance (and to highlight outstanding issues) prior to development of an accepted international central BP validation protocol. A list of issues in need of resolution in the future development of such a protocol is provided in Table 4.

Sample characteristics. A sample size of at least $n = 85$ adults is proposed based on brachial BP validation protocols and the requirement to detect a mean difference of 5 mmHg (standard deviation (S_d) of the difference 8 mmHg) with an estimated power of $>99\%$ (two-sided alpha of 5%), as currently proposed by the AAMI standard. Nevertheless, invasive BP measures during clinical procedures face additional constraints that can increase BP variability, such as selective patient characteristics and limited time for repeat measurements. Thus, a definitive sample size based on robust statistical methods is still needed. If devices are to be used in paediatric age groups, then wherever possible, accuracy should be tested separately in those groups and not extrapolated from adults. Participants

Table 3 Summary of central blood pressure (BP) device validation protocol components and requirements.

Protocol Section	Protocol Item	Protocol Requirement	Protocol Undertaken (circle yes/no comment)
Study setting	Isolated room without disturbing influences.	Should	YES NO.....
Non-invasive central BP device measurement standards	List manufacturer, model, software version, operating principles, signal processing step/s, calibration processes.	Must	YES NO.....
	Time for BP measures; time points of brachial BP and central BP; cuff deflation speed.	Should	YES NO.....
	Define and use appropriate cuff size.	Must	YES NO.....
	Dimensions of inflatable bladder for all cuff sizes available; process to determine cuff size.	Should	YES NO.....
	Process of familiarisation with equipment.	Should	YES NO.....
	Separate validation studies for additional or optional features or functions.	Must	YES NO.....
	Process/s of quality control; process used to delineate acceptable quality; number of unacceptable readings; reason/s for exclusion.	Must	YES NO.....
Invasive (intra-arterial) central BP reference standard	Micromanometer-tipped catheter used if minor inflection points to be identified.	Should	YES NO.....
	Full description of catheter; frequency response and handling procedures.	Must	YES NO.....
	Performance comparison of fluid filled catheter with micromanometer-tipped catheter.	May	YES NO.....
Data acquisition at rest	Period of undisturbed rest; medications used.	Should	YES NO.....
	No talking. Free from acute hemodynamic interventions	Must	YES NO.....
	Test device compared with reference over time-period matching the test device deflation cycle; recorded under stable conditions.	Must	YES NO.....
	Complete description of protocol; time interval between test device and reference measures.	Must	YES NO.....
Data acquisition at BP intervention	Hemodynamic change from resting state.	May	YES NO.....
	Description of the intervention procedure.	Must	YES NO.....

SBP, systolic BP; DBP, diastolic BP. Complete details of protocol components and requirements are contained within the body text of the original publication.²³ Must, necessary component for highest quality; Should, strong recommendation, but probably not the only way that the component can be achieved; May, further guidance required.

should have a sex distribution of at least 30% male and female and in sinus rhythm unless the device is being tested for accuracy during arrhythmias.²⁵ In keeping with all other brachial cuff BP validation guidelines, devices should be tested over a range of BP. An indicative range for invasive central SBP may be ≤ 100 mmHg ($\geq 5\%$ of readings), ≥ 140 mmHg ($\geq 20\%$ of readings) and ≥ 160 mmHg ($\geq 5\%$ of

readings), and the indicative range for invasive central DBP may be ≤ 60 mmHg ($\geq 5\%$ of readings), ≥ 85 mmHg ($\geq 20\%$ of readings) and ≥ 100 mmHg ($\geq 5\%$ of readings).²⁴ Device accuracy should also be tested across a range of heart rates (i.e. 60–100 bpm), because heart rate influences aortic stiffness and SBP amplification.^{32,33} Exact criteria for BP and heart rate ranges needs to be resolved. Unless testing

Table 4 Summary list of issues for consideration in development of an internationally accepted central blood pressure (BP) validation protocol.

Validation protocol features	Comments
<i>Reference method</i>	
Non-invasive reference standard.	What criteria needed to satisfy for an acceptable non-invasive alternative to the invasive method which restricts study sample characteristics?
<i>Error</i>	
Minimum standard.	What is the magnitude of the minimum acceptable error and its frequency based on the invasive reference standard?
<i>Study sample</i>	
Definition of general population sample.	Which populations should be considered as special as there may be different device measurement accuracy from the general population, and therefore require separate validation?
Minimum sample size for a general population study.	Based on the reference method for an acceptable statistical risk of false positive and negative results.
Sample size for validations in special groups.	To be defined after a successful study in the general population has been completed.
Sex and age distribution.	Representation of males and females, adolescents, young and middle aged adults and elderly.
BP and heart rate range criteria.	Based on reference central BP measurements and heart rate during the procedure?
Cuff size.	Minimum number of subjects investigated per different cuff size, or number of different cuffs to be studied in a single study?
Exclusion criteria.	On the basis of increased reference BP variation within individual validation procedures or clinical conditions.
<i>Procedural</i>	
Number of measurements.	Procedure for the number of reference and test BP measurements in a validation session.
Comparison with reference.	How to compare when operating characteristics differ between reference (i.e. beat-to-beat) and non-invasive test devices (i.e. averaging over seconds to minutes) and influence of respiratory variation and arrhythmias?
<i>Reporting</i>	
Data and pass criteria.	What data, statistics and study features to be reported? What pass/fail criteria?

device performance in specific cardiac or respiratory diseases, it should be noted that subjects with the following conditions have a higher likelihood of measurement error due to abnormal haemodynamics: severe valvular stenosis or regurgitation, severely impaired left ventricular systolic function, atrial fibrillation, constrictive pericarditis, pericardial tamponade, restrictive cardiomyopathy or severe pulmonary disease.

Statistical requirements. Beyond the reporting of details already mentioned, description of subjects must be presented and should include basic demographics (age, sex, ethnicity, body mass index), medications and clinical conditions including outcome of coronary catheterization procedure. Comparison between non-invasive and reference BP's must report mean difference, S_d of the mean difference, and limits of agreement (LOA), illustrated by modified Bland–Altman plots³⁴ in which the mean of measurements is replaced by the reference catheter measurement. Scatter plots of the measures obtained with the non-invasive device (on Y axis) versus the reference method (on X axis), with the line of equality, may also be provided for descriptive purposes. Non-uniformity of S_d across the range of measurement or evidence of non-constant bias (e.g. increasing difference between measures with increasing values) must be visually checked on the

Bland–Altman plots. An increase in variability of the differences as the magnitude of the measurement increases can be dealt with by log transformation of both measurements before analysis and the LOA derived from log transformed data should be reported after back-transformation (and thus expressed as ratios of the actual measurements). When log transformations do not solve the problem of a relationship between the difference and the mean, regression approaches or non-parametric approaches can be used instead, but with preference for the latter (for details see³⁴). Absolute BP differences from the reference should be presented as a clinically meaningful illustration of the results but without a pass/fail criteria.²⁴ The proposed pass criteria is if the device has a mean difference of ≤ 5 mmHg with $S_d \leq 8$ mmHg compared with the reference, based on the magnitude of minimum tolerable error and frequency,²⁴ but also recognizing this is a feature requiring resolution in future guidelines.

Conclusions and future directions

A major reason for producing this document to improve device validity has been the ongoing controversy over whether central BP adds prognostic value to that from

routine brachial cuff BP. A recent Framingham paper found no additional value,³⁵ while two systematic reviews not including those data came to opposite conclusions.^{14,36} For unfamiliar readers, an accompanying editorial addresses the issues.³⁷ A number of perceived deficits relating to both brachial and central BP measurement have been brought to attention in this current paper, and accordingly some points of intent require additional explanation. Firstly, despite the premise of clinical brachial BP measurement being based on essentially inaccurate cuff measures, brachial BP is still important and regarded as the clinical standard. This document should not be interpreted as challenging the clinical utility of brachial BP measurement, nor its value in hypertension management. Similarly, this document does not seek to undermine the potential clinical use of currently available non-invasive central BP devices that have not undergone the validation procedures recommended in this document, but have already proven to provide measurement of physiological (e.g. vascular ageing)³⁸ or prognostic significance. Nevertheless, with the advent of "precision medicine," clinical decisions are expected to be refined and improved by using more accurate BP monitors into the future, whether brachial or central BP, and this is a key research need. Additional guidance on central BP validation protocols is keenly awaited from regulatory authorities.

Conflict of interest

A.Avolio has received equipment for research from BPLab and AtCor Medical.

J.Blacher has received equipment for research projects from AtCor Medical.

C.Chen has received funding and equipment for research projects from Omron Corporation and Microlife Corporation.

P.Chowienzyk and King's College London have an interest in Centron Diagnostics.

J.Cockcroft has received equipment and travel grants from I.E.M. GmbH, Philips Healthcare.

I.Ferreira none.

A.Hughes has received loans of equipment from ALOKA/Hitachi Medical Systems, AtCor Medical, Finapres Medical Systems, I.E.M. GmbH, Philips Healthcare, Pulsecor Ltd, SpaceLabs/Dolby and USCOM.

B.McDonnell has received equipment from AtCor Medical and I.E.M. GmbH, Philips Healthcare.

S.Millasseau has received revenue from ALAM Medical, AtCor Medical, Omron and Esaote.

T.G.Papaioannou has received equipment from I.E.M. GmbH.

G.Parati has conducted validation studies for various manufacturers.

J.Park has received equipment for research projects from Fukuda Denshi.

A.Protogerou has received funding and equipment for research projects from AtCor Medical and I.E.M. GmbH.

M.Roman none.

P.Segers has received equipment for research projects from Fukuda Denshi.

G.Stergiou has conducted validation studies for various manufacturers; advised manufacturers on device development.

G.Schillaci has received funding and equipment for research projects from AtCor Medical and I.E.M. GmbH, Philips Healthcare.

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James E. Sharman*

Menzies Institute for Medical Research, University of Tasmania, Hobart, Australia

Alberto P. Avolio

Department of Biomedical Sciences, Faculty of Medicine and Health Sciences, Macquarie University, Sydney, Australia

Johannes Baulmann
*Clinic of Internal Medicine II, University Hospital
 Schleswig-Holstein, Luebeck, Germany*

Athanase Benetos
*Département de Médecine Gériatrique, CHRU de Nancy,
 INSERM U1116, Université de Lorraine, Vandoeuvre-les-
 Nancy, France*

Jacques Blacher
*Hypertension and Cardiovascular Prevention Unit, Hôtel-
 Dieu University Hospital, Assistance Publique-Hôpitaux de
 Paris, University Paris Descartes, Paris, France*

C. Leigh Blizzard
*Menzies Institute for Medical Research, University of
 Tasmania, Hobart, Australia*

Pierre Boutouyrie
*Departments of Pharmacology, European Georges
 Pompidou Hospital, Assistance Publique Hôpitaux de Paris,
 Inserm UMR 970 and University Paris Descartes, Paris,
 France*

Chen-Huan Chen
*Department of Medicine, Faculty of Medicine, National
 Yang-Ming University, Taipei, Taiwan, ROC*

Phil Chowienzyk
*Department of Clinical Pharmacology, King's College
 London British Heart Foundation Centre, UK*

John R. Cockcroft
*Department of Biomedical Sciences, School of Health
 Sciences, Cardiff Metropolitan University, Cardiff, UK*

J. Kennedy Cruickshank
*Cardiovascular Medicine Group, Division of Diabetes and
 Nutritional Sciences, King's College, London, UK*

Isabel Ferreira
*The University of Queensland, School of Public Health,
 Herston, Brisbane, Australia*

Lorenzo Ghiadoni
*Department of Clinical and Experimental Medicine,
 University of Pisa, Pisa, Italy*

Alun Hughes
*Institute of Cardiovascular Science, University College
 London, UK*

Piotr Jankowski
*First Department of Cardiology and Hypertension, Institute
 of Cardiology, Jagiellonian University Medical College,
 Poland*

Stephane Laurent
*Departments of Pharmacology, European Georges
 Pompidou Hospital, Assistance Publique Hôpitaux de Paris,*

*Inserm UMR 970 and University Paris Descartes, Paris,
 France*

Barry J. McDonnell
*Department of Biomedical Sciences, School of Health
 Sciences, Cardiff Metropolitan University, Cardiff, UK*

Carmel McEniery
*Division of Experimental Medicine and
 Immunotherapeutics, Department of Medicine, University
 of Cambridge, Cambridge, UK*

Sandrine C. Millasseau
Pulse Wave Consulting, Saint Leu la Foret, France

Theodoros G. Papaioannou
*Biomedical Engineering Unit, First Department of
 Cardiology, Hippokraton Hospital, Medical School,
 National and Kapodistrian University of Athens,
 Greece*

Gianfranco Parati
*Department of Cardiology, S.Luca Hospital, Istituto
 Auxologico Italiano, Department of Medicine and Surgery,
 University of Milano-Bicocca, Milan, Italy*

Jeong Bae Park
*Department of Medicine/Cardiology, Cheil General
 Hospital, Dankook University College of Medicine, Seoul,
 Republic of Korea*

Athanase D. Protogerou
*Cardiovascular Prevention and Research Unit, Department
 of Pathophysiology, 'Laiko' Hospital, Medical School,
 National and Kapodistrian University of Athens,
 Greece*

Mary J. Roman
*Division of Cardiology, Department of Medicine, Weill
 Cornell Medical College, New York, NY, USA*

Giuseppe Schillaci
*Dipartimento di Medicina, Università di Perugia, Unità di
 Medicina Interna, Ospedale 'S. Maria', Terni, Italy*

Patrick Segers
IBiTech-bioMMeda, Ghent University, Ghent, Belgium

George S. Stergiou
*Hypertension Center STRIDE-7, National and Kapodistrian
 University of Athens, Third Department of Medicine,
 Sotiria Hospital, Athens, Greece*

Hirofumi Tomiyama
*Department of Cardiology, Tokyo Medical University,
 Tokyo, Japan*

Raymond R. Townsend
*Perelman School of Medicine, University of Pennsylvania,
 Philadelphia, PA, USA*

Luc M. Van Bortel
*Heymans Institute of Pharmacology, Ghent University,
Ghent, Belgium*

Jiguang Wang
*The Shanghai Institute of Hypertension, Ruijin Hospital,
Shanghai Jiaotong University School of Medicine, Shanghai,
China*

Siegfried Wassertheurer
*Austrian Institute of Technology, Health & Environment
Department, Vienna, Austria*

Thomas Weber
*Cardiology Department, Klinikum Wels-Grieskirchen, Wels,
Austria*

Ian B. Wilkinson
*Division of Experimental Medicine and
Immunotherapeutics, Department of Medicine, University
of Cambridge, Cambridge, UK*

Charalambos Vlachopoulos
*First Department of Cardiology, Hippokration Hospital,
Medical School, National and Kapodistrian University of
Athens, Greece*

*Corresponding author. Menzies Institute for Medical
Research, University of Tasmania, Hobart, Australia.

E-mail address: james.sharman@utas.edu.au

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